





Department of Physics

REC3D

An Accumulative Reconstruction Algorithm based on Volume Intersectional Information for PET

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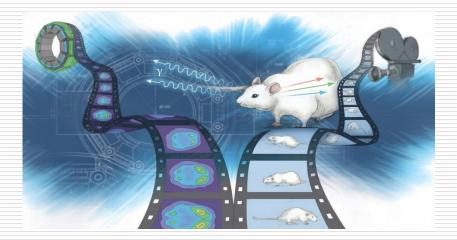
Outline

Introduction



- Gate Simulations
 - Cylinder Phantoms
 - Parallel Plate PEM

Conclusions



Reconstruction Algorithms



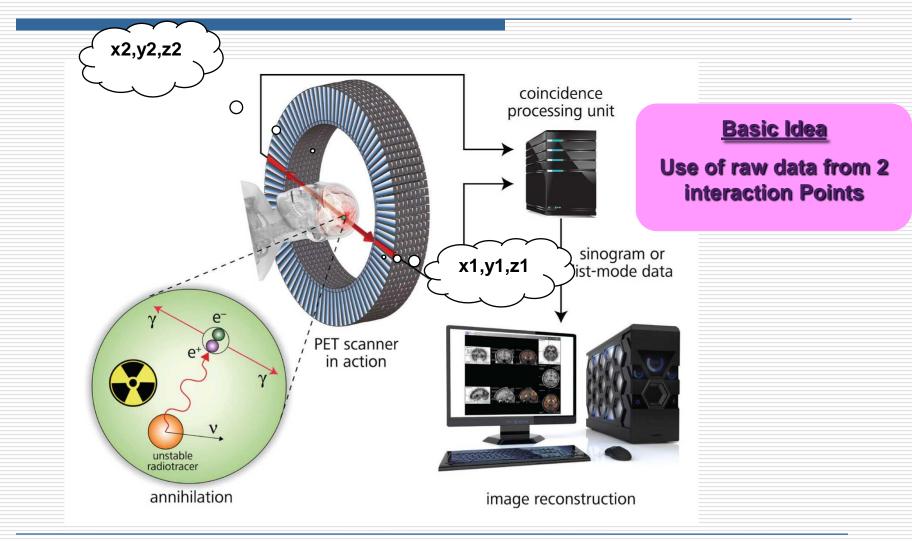


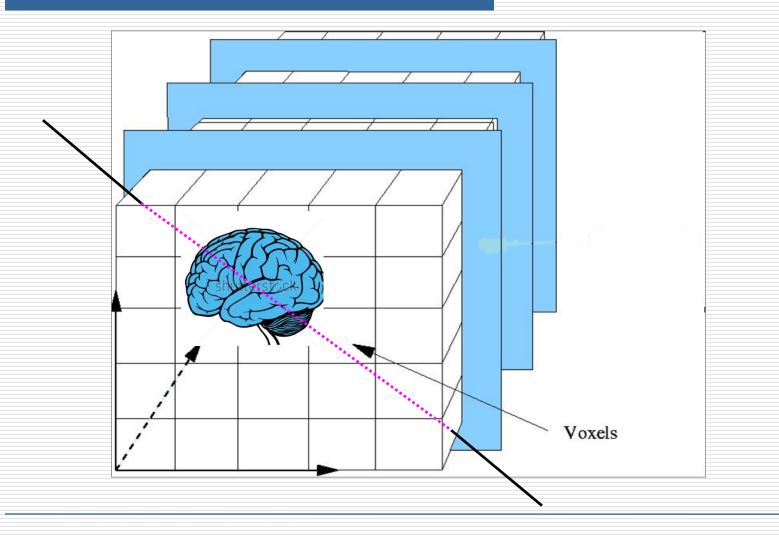
A Fourier Transformation is used, which is like Randon Transformation for X-rays.

$$\mathbf{F}(\mathbf{k}_{x},\mathbf{k}_{y}) = \int_{-\infty-\infty}^{+\infty+\infty} \mathbf{f}(x,y) e^{-2\pi i (x\mathbf{k}_{x}+y\mathbf{k}_{y})} dxdy$$

ITTERATIVE ALGORITHMS OSEM,MLEM

$$\lambda_i^{new} = \frac{\lambda_i^{old}}{p_i} \sum_{j}^{N_i} \frac{n_j^* p_{ij}}{\sum_{k}^{N} \lambda_k^{old} p_{kj}}$$





For a certain Z plane and two points P1(x1,y1,z1), P2(x2,y2,z2) the line that will intersects the plane is given by the equation :

$$\frac{x - x_1}{x_2 - x_1} = \frac{y - y_1}{y_2 - y_1} = \frac{z - z_1}{z_2 - z_1}$$

The intersection point is given by:

$$\mathbf{x}_{n} = \frac{\mathbf{Z}_{0} - \mathbf{Z}_{1}}{\mathbf{Z}_{2} - \mathbf{Z}_{1}} \bullet (\mathbf{X}_{2} - \mathbf{X}_{1}) + \mathbf{X}_{1}$$
$$\mathbf{y}_{n} = \frac{\mathbf{Z}_{0} - \mathbf{Z}_{1}}{\mathbf{Z}_{2} - \mathbf{Z}_{1}} \bullet (\mathbf{Y}_{2} - \mathbf{Y}_{1}) + \mathbf{Y}_{1}$$

Euclidean distance that the line has traversed in each voxel is:

Dis =
$$\sqrt{(x_{B} - x_{A})^{2} + (y_{B} - y_{A})^{2} + (z_{B} + z_{A})^{2}}$$

The distance **Dis** is basically an accumulative weight factor, which is used to assign the luminosity distribution in each voxel.

Total Number of steps : N³

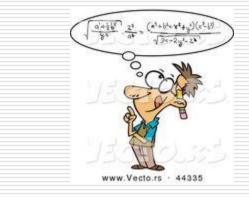
x_B,y_B,z_B

 $\mathbf{X}_{A}, \mathbf{Y}_{A}, \mathbf{Z}_{A}$

Accelerated image Reconstruction

Instead of scanning the whole voxelized Volume in order to save computation time and having Dis already calculated we make a step further to calculate the first Derivative :

$$- DivX = \frac{C_{2x} - C_{1x}}{De}$$
$$- DivY = \frac{C_{2y} - C_{1y}}{De}$$
$$- DivZ = \frac{C_{2z} - C_{1z}}{De}$$



This way we can "predict" the path of the LOR inside the Volume.

Accelerated image Reconstruction

In order to insure high accuracy we introduce a specific step to the calculation of the derivative.

$$QQ(1) = C_1(1) + 0.01 * x_{step} * DivX$$
$$QQ(2) = C_1(2) + 0.01 * y_{step} * DivY$$
$$QQ(3) = C_1(3) + 0.01 * z_{step} * DivZ$$



QQ(1),QQ(2),QQ(3) are the intersection points of the LOR inside every voxel and xstep, ystep, zstep insure that during the Div calculation we stay inside the voxel.

Accelerated image Reconstruction

The total number of steps in this method is :

Max Total Steps:
$$\sqrt{N_x^2 + N_y^2 + N_z^2}$$

To compare the two methodos :

$$rac{N^3}{N\sqrt{3}} pprox rac{N^2}{2}$$



The factor N²/2 is translated to less computation time

Evaluation of REC3D

In order to evaluate the effectiveness of Rec3D we made:

- ✓ Gate simulations of two different type of Scanners.
- ✓ Evaluation of Image Reconstruction.

Comparison between REC3D and commercially available programs.

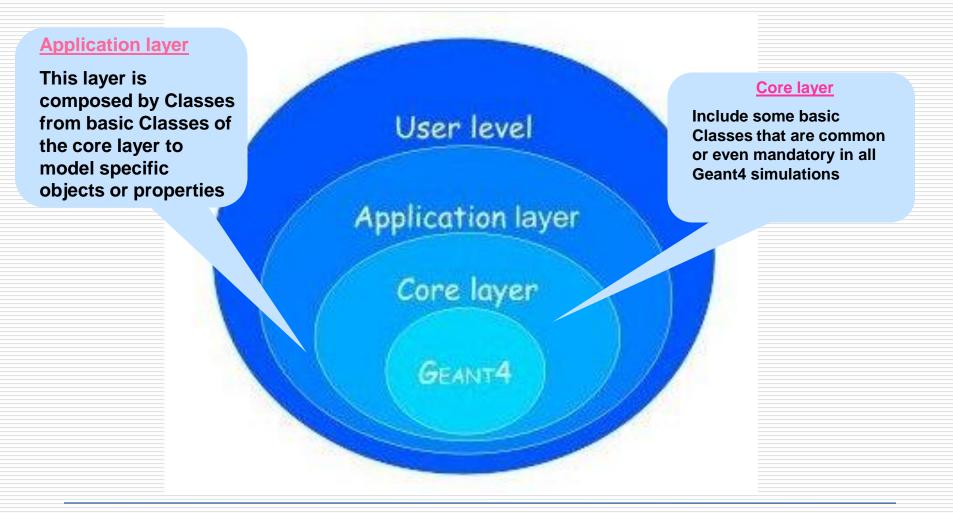
GATE

Gate, the Geant4 Application for Tomographic Emission, combines the advantages of the generalpurpose Geant4 simulation code and of specific software tool implementations dedicated to emission tomography.

Indeed, GATE takes advantage of the well-validated physics models, of the geometry description, and of the visualization and 3D rendering tools offered by Geant4 but has a distinctive characteristic the modeling of time-dependent processes.







Cylindrical PET Simulation

Sherbrooke 16 ring PET		
Outer Diameter	190 mm	
Inner Diameter	150 mm	
Height	40 mm	
Crystal	BGO	
Crystal size	20X3X3 mm ³	
Total Number of Crystals per ring	256	
Number of rings	16	

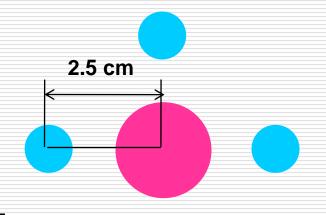
Source Features

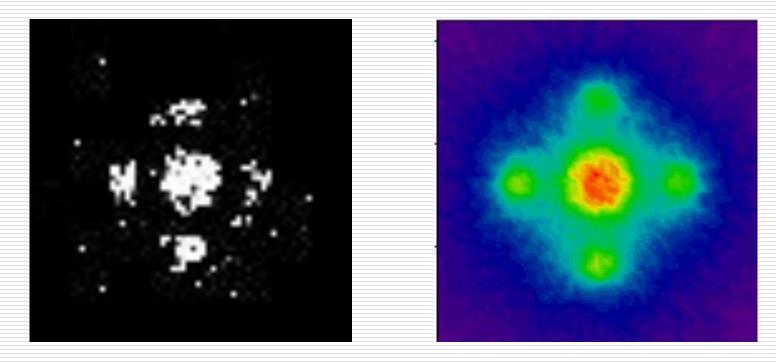
Simulation 1

- Source Activity: 10 kBq
- Type: Cylinder
- Number: 5

PET: Sherbrooke 16rings

# Source	Radius	Height	Туре	
0	1 cm	32 mm	γ	
1	0.5 cm	8 mm	γ	
2	0.5 cm	16 mm	γ	
3	0.5 cm	24 mm	γ	
4	0.5 cm	32 mm	γ	

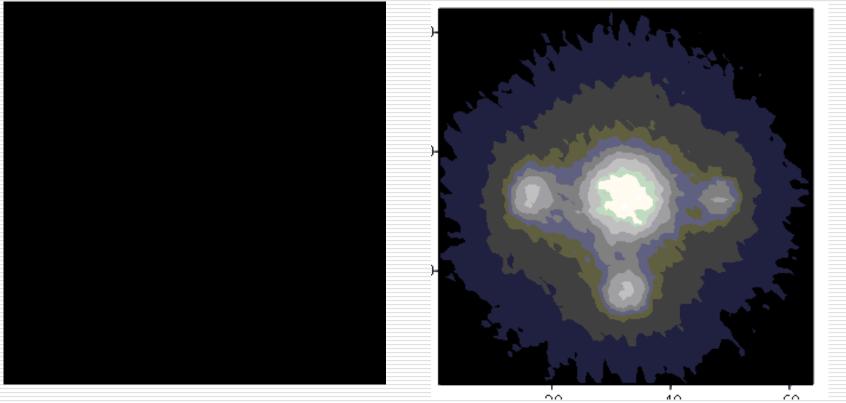




OSEM

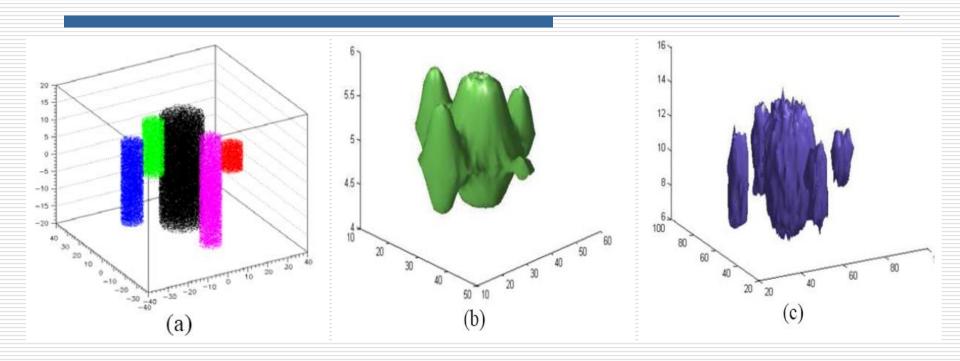


Sherbrooke 16ring PET







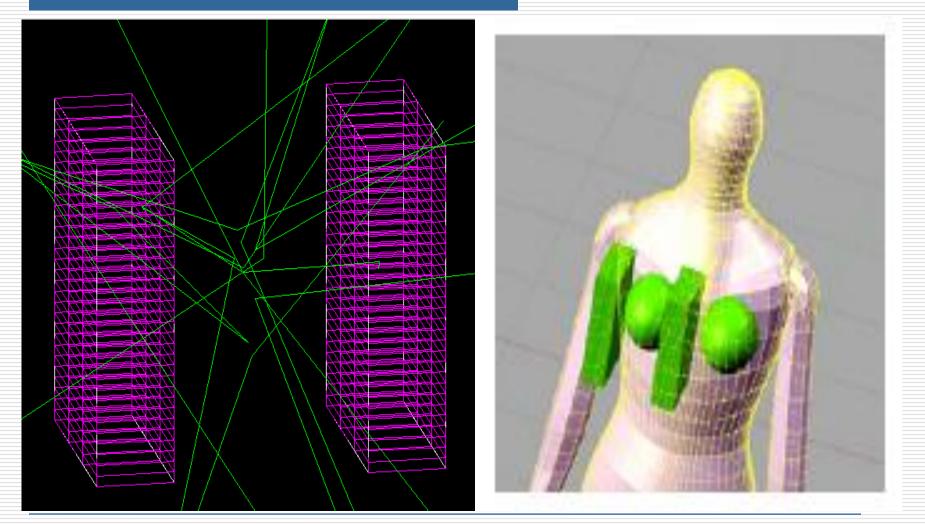


(a) Five Cylinder Simulation Phantom(b) Reconstruction with Non-Energy Cut(c) Reconstruction with Energy Cut

Sherbrooke 16ring PET





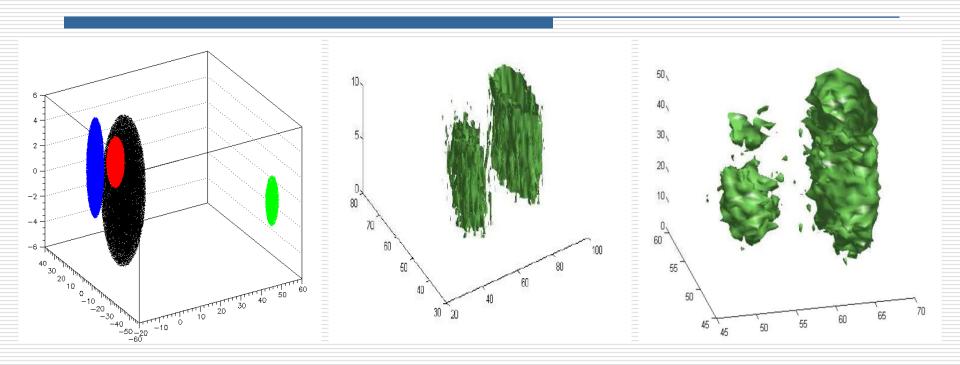


Design study of a high-resolution breast dedicated PET system built from CZT detectors

Hao Peng and Craig S. Levin

Simulation Features

		Simulation 2						
Number of Plates	2	 Source Activity: 10 kBq Type: Ellipse 						
Plate dimension	12X15X4 cm	 Number: 4 PEM 						
Crystal dimension	4X0.5X4 cm							
		#	a=b(mm)	c (mm)	x,y,z	Туре		
Number of Crystals	2)/20)/4							
in X axis, Y axis, Z axis	3X30X1	1	10	6	0,0,0	Y		
Type of Crystal CZT	2	4	4	30,0,0	Y			
	3	4	2	30,10,0	Y			
		4	3	2	-50,50,0	γ		



- (a) Four Ellipse Simulation Phantom
- (b) Reconstruction with Non-Energy Cut
- (c) Reconstruction with Energy Cut

Conclusions

REC3D

- Efficient reconstruction without artifacts
- The Real Scanning Range is defined by the user.
- The number of voxels in x,y,z axis is defined by the user.
- Can be used for any scanner geometry.
- Introduction of energy cut.
- User Friendly.



ΣΑΣ ΕΥΧΑΡΙΣΤΩ ③



Γεωμετρικά Χαρακτηριστικά

